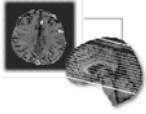


Neuroscience 2004 Functional Brain Imaging



*Joy Hirsch, Ph.D., Professor
Director, fMRI Research Center
Columbia University Health Sciences
NI Basement*

www.fmri.org

Columbia fMRI

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A Brief Outline

I. Hypothesis of functional specificity

- A. Single Areas
- B. Multiple Areas

II. Brain Mapping Techniques

- A. Lesion- Based Methods
 - 1. Positron Emission Tomography, PET
 - 2. Functional Magnetic Resonance Imaging, fMRI
- B. Cardiovascular Based Methods
 - 1. Positron Emission Tomography, PET
 - 2. Functional Magnetic Resonance Imaging, fMRI
- C. Electromagnetic-Based Methods
 - 1. SSEP Somatosensory Potentials
 - 2. Cortical Stimulation
 - 3. Magnetoencephalography, MEG
 - 4. Electroencephalography, EEG

III. Integration of Brain Mapping Techniques

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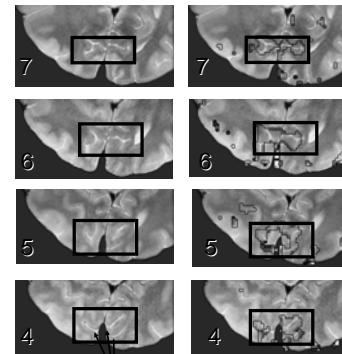
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I. Hypothesis of functional specificity Specializations of single brain areas

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Primary
Visual Cortex



Flashing
LED Display

Calcarine Sulcus

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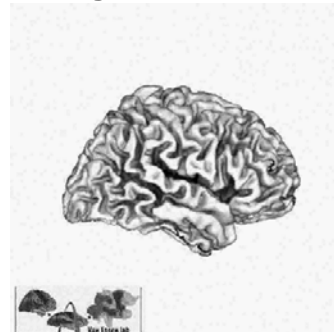
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I. Hypothesis of functional specificity Specializations of single brain areas Specializations of multiple brain areas

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Functional Organization of Visual Cortex



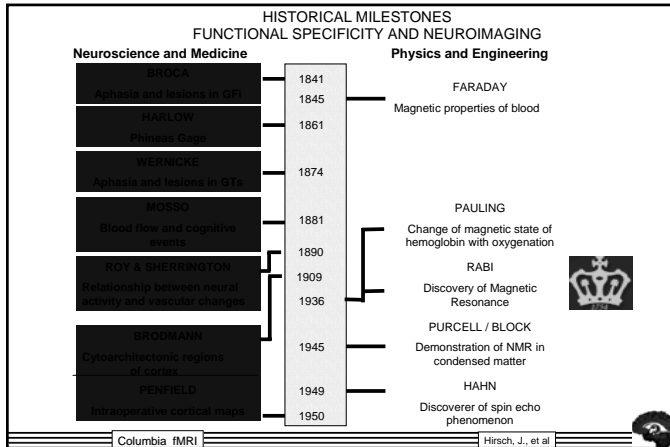
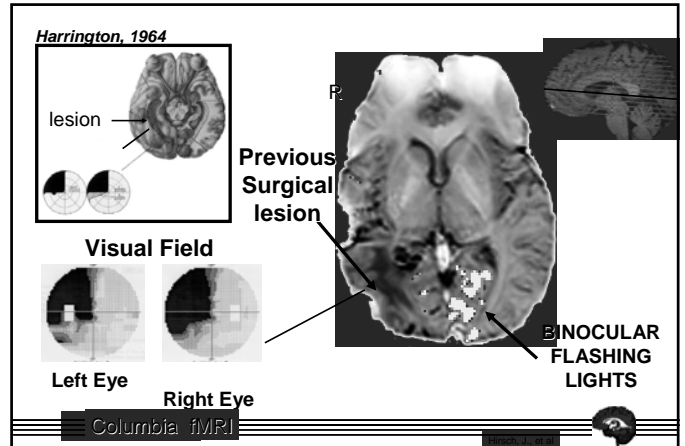
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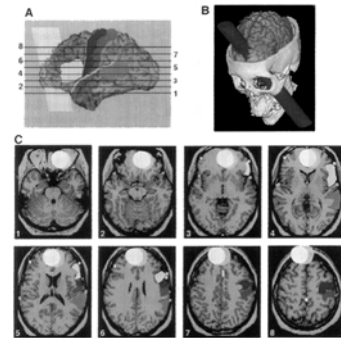
II. Brain Mapping Techniques

A. Lesion-Based Methods

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Phineas Gage

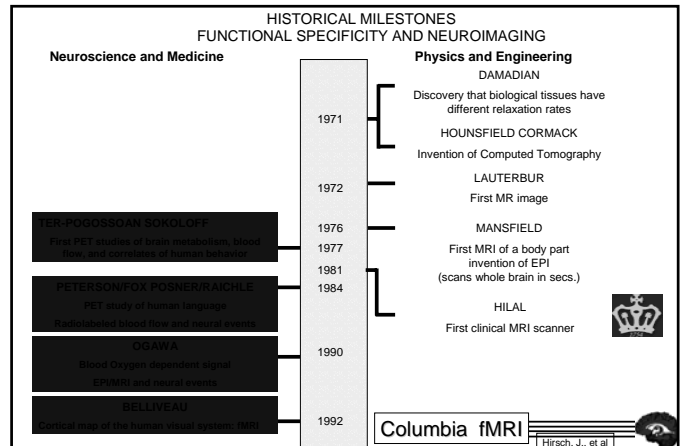


II. Brain Mapping Techniques

B. Cardiovascular Based Methods

1. Positron Emission Tomography, PET

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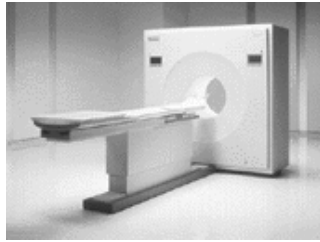


a. Source of Signal Positron Emission Tomography

Radionuclides that emit positrons such as ^{15}O and ^{18}F are introduced into the brain.

H_2^{15}O behaves like H_2^{16}O and indicates blood flow (rCBF) (half life = 123 seconds) integration time ≈ 60 seconds.

^{18}F - deoxyglucose behaves like deoxyglucose and indicates metabolic activity (half-life = 110 minutes) integration time ≈ 20 minutes



PET SCANNER

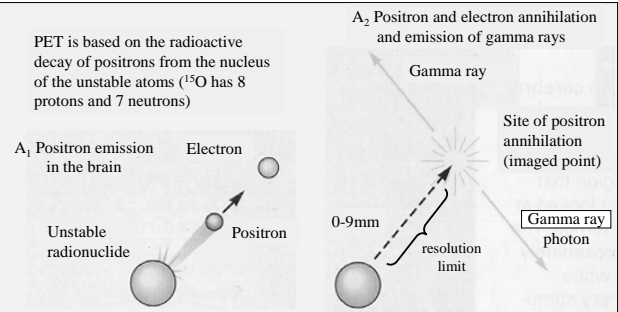
From: www.epub.org.br/cm/n011pet/pet.htm

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Principle of PET

PET is based on the radioactive decay of positrons from the nucleus of the unstable atoms (^{15}O has 8 protons and 7 neutrons)



From: Principles of Neural Science (4th. Ed.) Kandel, Schwartz, & Jessell, p. 377.

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II. Brain Mapping Techniques

B. Cardiovascular Based Methods

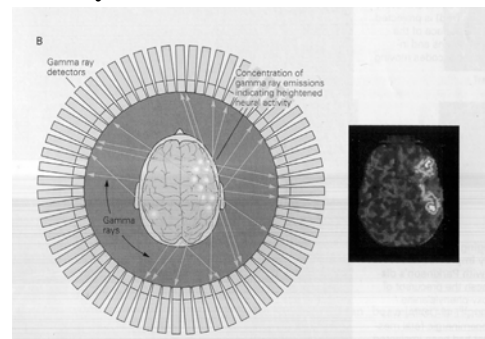
1. Positron Emission Tomography, PET

- a. Source of signal
- b. Measurement techniques

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Gamma Ray Detections to Location of Function



From: Principles of Neural Science (4th. Ed.) Kandel, Schwartz, & Jessell, p. 377.

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Injection of radioactive-labeled water for PET scanning



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II. Brain Mapping Techniques

B. Cardiovascular Based Methods

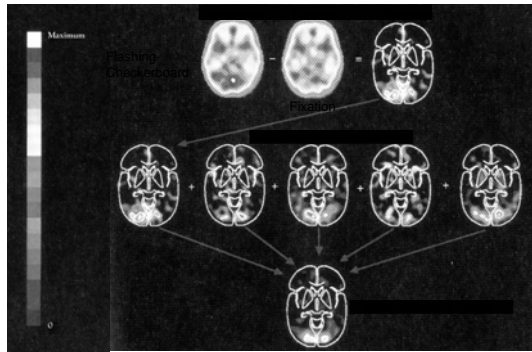
1. Positron Emission Tomography, PET

- a. Source of signal
- b. Measurement techniques
- c. Computation for analysis

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Analysis of PET Results



From: Images of Mind by Posner, M. and Raichle, M. Scientific American Library, 1994, p. 24

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II. Brain Mapping Techniques

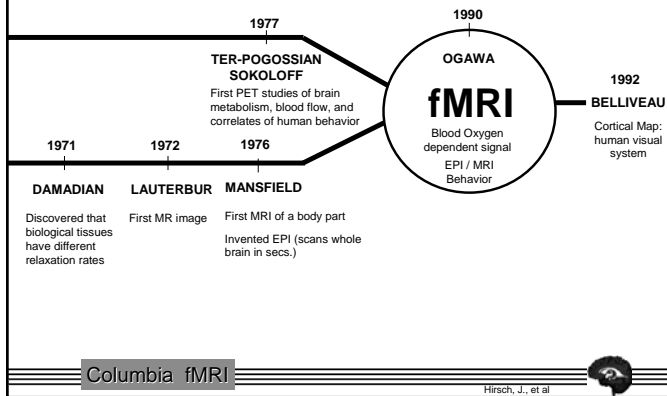
B. Cardiovascular Based Methods

1. Positron Emission Tomography, PET
2. Functional Magnetic Resonance Imaging, fMRI

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HISTORICAL MILESTONES



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II. Brain Mapping Techniques

1. Functional Magnetic Resonance Imaging, fMRI

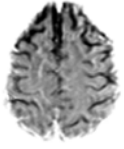
a. Source of signal

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a. Source of Signal Principles of fMRI

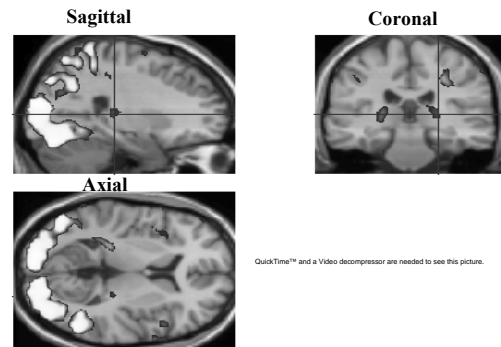
The MR Signal and 4 Magnetic Fields

| | | |
|---|---|---|
|  | MAGNETIC FIELD 1: <ul style="list-style-type: none"> ◦Scanner Environment [1.5] T ◦Protons align along an axis | MAGNETIC FIELD 2: <ul style="list-style-type: none"> • Created when a radio frequency pulse (63.3 mgHz) is applied • Protons precess around the axis and create a small current (MRI signal) • Protons return to aligned state when radio frequency pulse is turned off |
| | MAGNETIC FIELD 3: <ul style="list-style-type: none"> • Location of the MR signal • A detectable radio frequency is emitted by the protons as they relax into their aligned state • The frequency is dependent upon field strength • Application of magnetic field gradient (mT) is sufficient to convert detected frequencies to location | MAGNETIC FIELD 4: <ul style="list-style-type: none"> • Local signal change at a single voxel is due to change in proportions of oxyhemoglobin/deoxyhemoglobin • Deoxyhemoglobin is paramagnetic and reduces the uniformity of the precessing and therefore the signal intensity • This change is called BOLD |

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Vision-related cortical effects

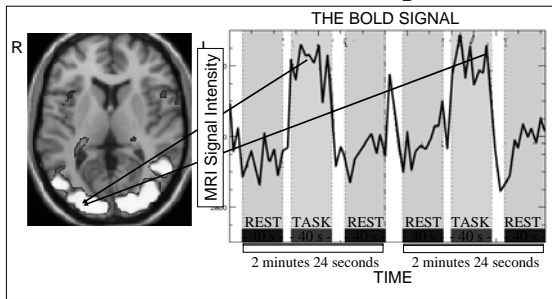


QuickTime™ and a Video decompressor are needed to see this picture.

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Current Developments in MR are focused on the structure/function problem



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PHYSIOLOGY

NEURAL ACTIVATION IS ASSOCIATED WITH AN INCREASE IN BLOOD FLOW

O₂ EXTRACTION IS RELATIVELY UNCHANGED

RESULT: REDUCTION IN THE PROPORTION OF DEOXY HGB IN THE LOCAL VASCULATURE

PHYSICS

DEOXY HGB IS PARAMAGNETIC

AND DISTORTS THE LOCAL MAGNETIC FIELD CAUSING SIGNAL LOSS

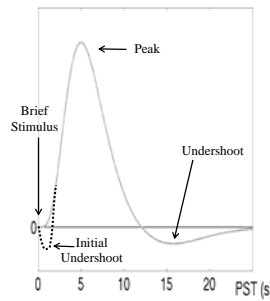
RESULT: LESS DISTORTION OF THE MAGNETIC FIELD RESULTS IN LOCAL SIGNAL INCREASE

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BOLD Impulse Response Model

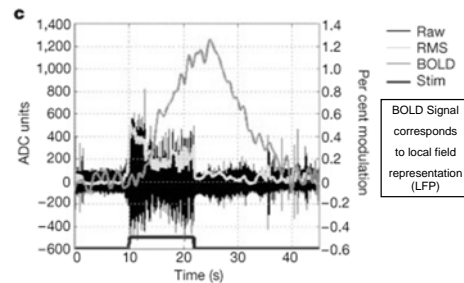
- Function of blood oxygenation, flow, volume (Buxton et al, 1998)
- Peak (max. oxygenation) 4-6s poststimulus; baseline after 20-30s
- Initial undershoot can be observed (Malonek & Grinvald, 1996)
- Similar across V1, A1, S1...
- ... but differences across other regions (Schacter et al 1997) individuals (Aguirre et al, 1998)



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BOLD ORIGIN



Logothetis, N.K., Pauls, , Angath, M, Torsten, T, Oeltermann, A, (2001) Neurophysiological investigation of the basis of the fMRI signal. Nature 412 158-157

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II. Brain Mapping Techniques

B. Cardiovascular Based Methods

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Imaging While Naming Objects



QuickTime™ and a Video decompressor are needed to see this picture.

QuickTime™ and a Radius SoftDV™ - NTSC decompressor are needed to see this picture.

Scanner acquires the whole brain every [4] secs:

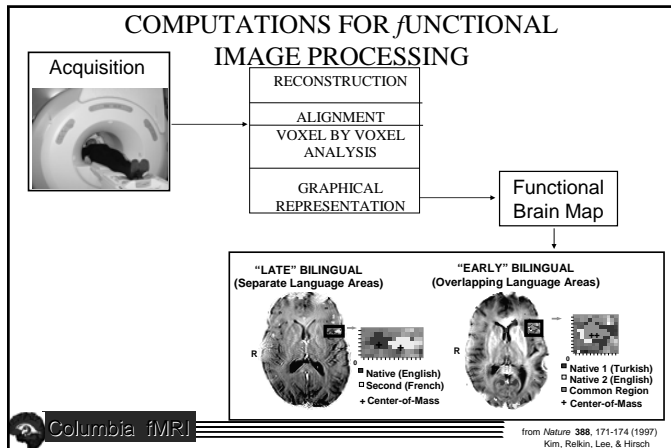
[26] axial slices

Resolution [1.5 x 1.5 x 4.5] mm

Each voxel is analyzed separately

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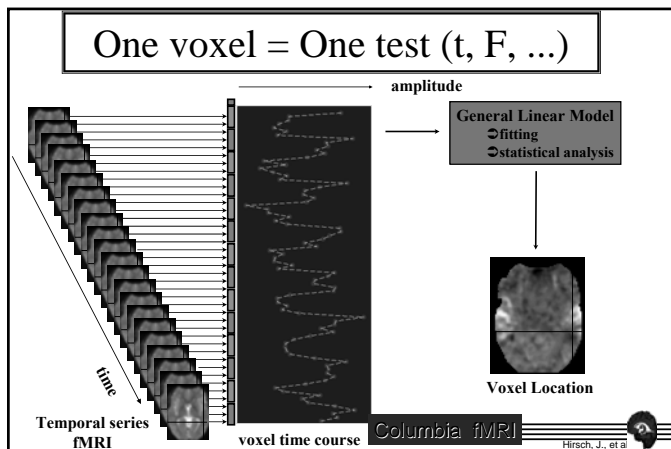
Block Design

| Time (sec) | Time (min) | Stage # | Task | Stage |
|------------|------------|---------|------|-------|
| 100 | 1:30 | 1 | Rest | 1 |
| 110 | 1:40 | 1 | Rest | 1 |
| 120 | 1:50 | 1 | Rest | 1 |
| 130 | 2:00 | 1 | Rest | 1 |
| 140 | 2:10 | 1 | Rest | 1 |
| 150 | 2:20 | 1 | Rest | 1 |
| 160 | 2:30 | 1 | Rest | 1 |
| 170 | 2:40 | 1 | Rest | 1 |
| 180 | 2:50 | 1 | Rest | 1 |
| 190 | 3:00 | 1 | Rest | 1 |
| 200 | 3:10 | 1 | Rest | 1 |
| 210 | 3:20 | 1 | Rest | 1 |
| 220 | 3:30 | 1 | Rest | 1 |
| 230 | 3:40 | 1 | Rest | 1 |
| 240 | 3:50 | 1 | Rest | 1 |
| 250 | 4:00 | 1 | Rest | 1 |
| 260 | 4:10 | 1 | Rest | 1 |
| 270 | 4:20 | 1 | Rest | 1 |
| 280 | 4:30 | 1 | Rest | 1 |
| 290 | 4:40 | 1 | Rest | 1 |
| 300 | 4:50 | 1 | Rest | 1 |
| 310 | 5:00 | 1 | Rest | 1 |
| 320 | 5:10 | 1 | Rest | 1 |
| 330 | 5:20 | 1 | Rest | 1 |
| 340 | 5:30 | 1 | Rest | 1 |
| 350 | 5:40 | 1 | Rest | 1 |
| 360 | 5:50 | 1 | Rest | 1 |
| 370 | 6:00 | 1 | Rest | 1 |
| 380 | 6:10 | 1 | Rest | 1 |
| 390 | 6:20 | 1 | Rest | 1 |
| 400 | 6:30 | 1 | Rest | 1 |
| 410 | 6:40 | 1 | Rest | 1 |
| 420 | 6:50 | 1 | Rest | 1 |
| 430 | 7:00 | 1 | Rest | 1 |
| 440 | 7:10 | 1 | Rest | 1 |
| 450 | 7:20 | 1 | Rest | 1 |
| 460 | 7:30 | 1 | Rest | 1 |
| 470 | 7:40 | 1 | Rest | 1 |
| 480 | 7:50 | 1 | Rest | 1 |
| 490 | 8:00 | 1 | Rest | 1 |
| 500 | 8:10 | 1 | Rest | 1 |
| 510 | 8:20 | 1 | Rest | 1 |
| 520 | 8:30 | 1 | Rest | 1 |
| 530 | 8:40 | 1 | Rest | 1 |
| 540 | 8:50 | 1 | Rest | 1 |
| 550 | 9:00 | 1 | Rest | 1 |
| 560 | 9:10 | 1 | Rest | 1 |
| 570 | 9:20 | 1 | Rest | 1 |
| 580 | 9:30 | 1 | Rest | 1 |
| 590 | 9:40 | 1 | Rest | 1 |
| 600 | 9:50 | 1 | Rest | 1 |
| 610 | 10:00 | 1 | Rest | 1 |
| 620 | 10:10 | 1 | Rest | 1 |
| 630 | 10:20 | 1 | Rest | 1 |
| 640 | 10:30 | 1 | Rest | 1 |
| 650 | 10:40 | 1 | Rest | 1 |
| 660 | 10:50 | 1 | Rest | 1 |
| 670 | 11:00 | 1 | Rest | 1 |
| 680 | 11:10 | 1 | Rest | 1 |
| 690 | 11:20 | 1 | Rest | 1 |
| 700 | 11:30 | 1 | Rest | 1 |
| 710 | 11:40 | 1 | Rest | 1 |
| 720 | 11:50 | 1 | Rest | 1 |
| 730 | 12:00 | 1 | Rest | 1 |
| 740 | 12:10 | 1 | Rest | 1 |
| 750 | 12:20 | 1 | Rest | 1 |
| 760 | 12:30 | 1 | Rest | 1 |
| 770 | 12:40 | 1 | Rest | 1 |
| 780 | 12:50 | 1 | Rest | 1 |
| 790 | 13:00 | 1 | Rest | 1 |
| 800 | 13:10 | 1 | Rest | 1 |
| 810 | 13:20 | 1 | Rest | 1 |
| 820 | 13:30 | 1 | Rest | 1 |
| 830 | 13:40 | 1 | Rest | 1 |
| 840 | 13:50 | 1 | Rest | 1 |
| 850 | 14:00 | 1 | Rest | 1 |
| 860 | 14:10 | 1 | Rest | 1 |
| 870 | 14:20 | 1 | Rest | 1 |
| 880 | 14:30 | 1 | Rest | 1 |
| 890 | 14:40 | 1 | Rest | 1 |
| 900 | 14:50 | 1 | Rest | 1 |
| 910 | 15:00 | 1 | Rest | 1 |
| 920 | 15:10 | 1 | Rest | 1 |
| 930 | 15:20 | 1 | Rest | 1 |
| 940 | 15:30 | 1 | Rest | 1 |
| 950 | 15:40 | 1 | Rest | 1 |
| 960 | 15:50 | 1 | Rest | 1 |
| 970 | 16:00 | 1 | Rest | 1 |
| 980 | 16:10 | 1 | Rest | 1 |
| 990 | 16:20 | 1 | Rest | 1 |
| 1000 | 16:30 | 1 | Rest | 1 |

Event-Related Design

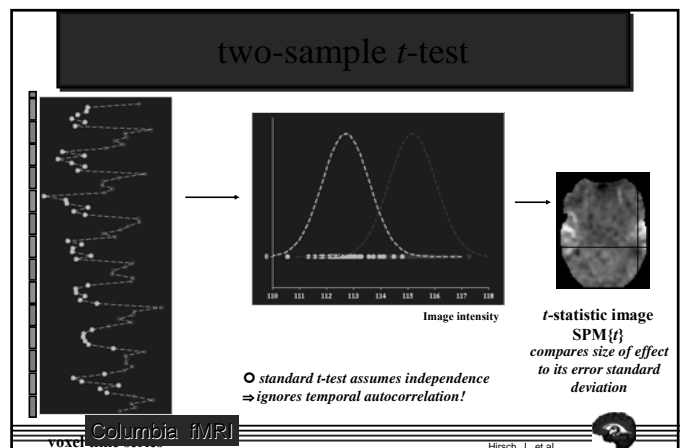
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| 830 | 13:40 | 1 | Rest | 1 |
| 840 | 13:50 | 1 | Rest | 1 |
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| 860 | 14:10 | 1 | Rest | 1 |
| 870 | 14:20 | 1 | Rest | 1 |
| 880 | 14:30 | 1 | Rest | 1 |
| 890 | 14:40 | 1 | Rest | 1 |
| 900 | 14:50 | 1 | Rest | 1 |
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| 940 | 15:30 | 1 | Rest | 1 |
| 950 | 15:40 | 1 | Rest | 1 |
| 960 | 15:50 | 1 | Rest | 1 |
| 970 | 16:00 | 1 | Rest | 1 |
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| 990 | 16:20 | 1 | Rest | 1 |
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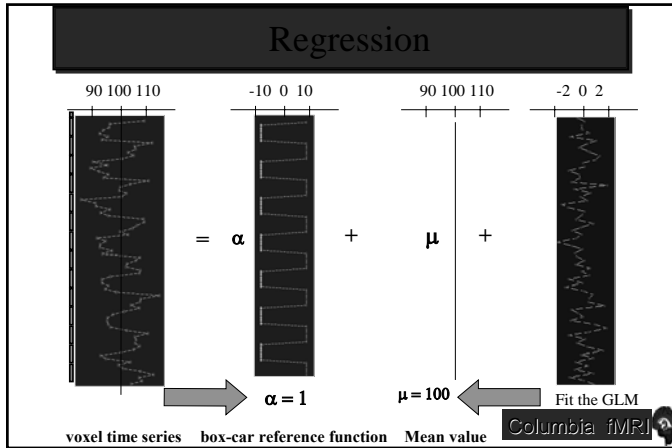
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- ## II. Brain Mapping Techniques
- ### B. Cardiovascular Based Methods
1. Positron Emission Tomography, PET
 2. Functional Magnetic Resonance Imaging, fMRI
 - a. Source of signal
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 - c. Computation for analysis
- Columbia fMRI

- ### Voxel statistics...
- parametric
 - one sample *t*-test
 - two sample *t*-test
 - paired *t*-test
 - Anova
 - AnCova
 - correlation
 - linear regression
 - multiple regression
 - *F*-tests
 - etc...
- } all cases of the
General Linear Model
assume normality
to account for serial correlations:
- Columbia fMRI



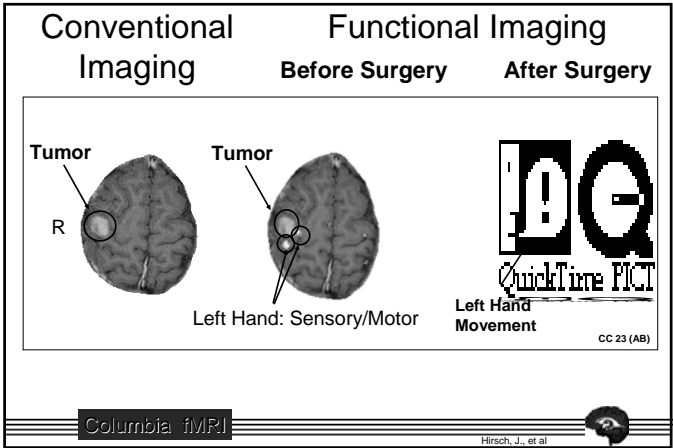
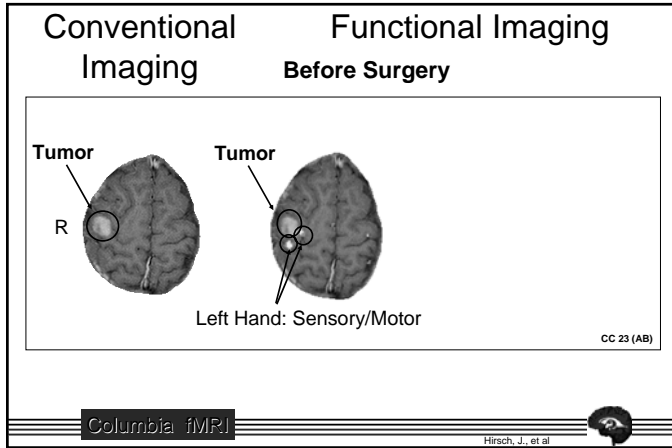
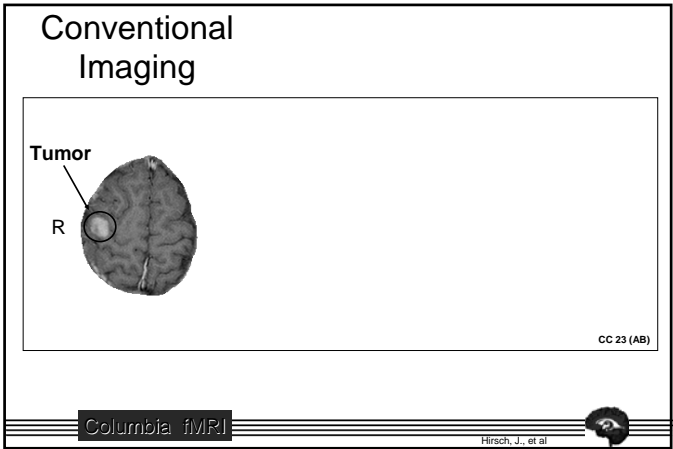


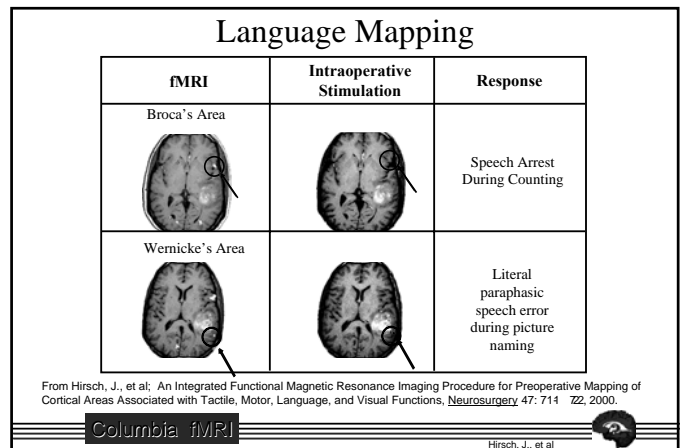
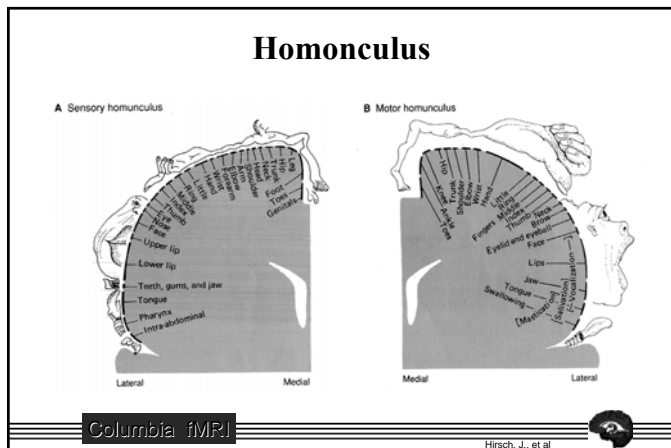
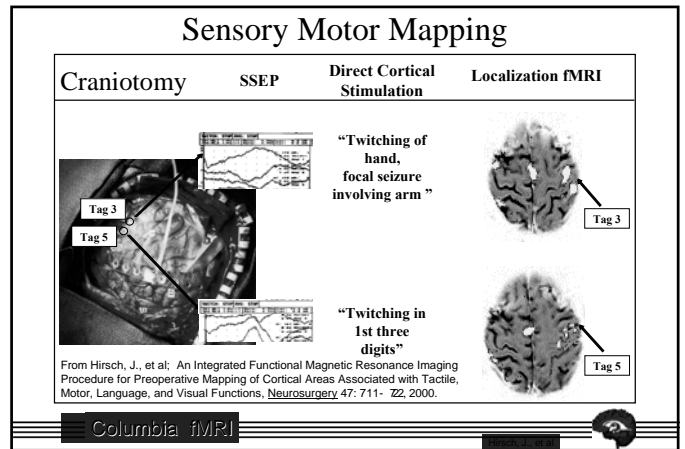
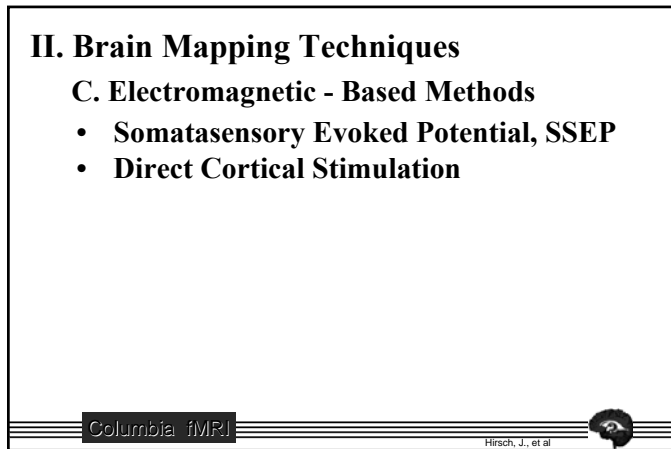
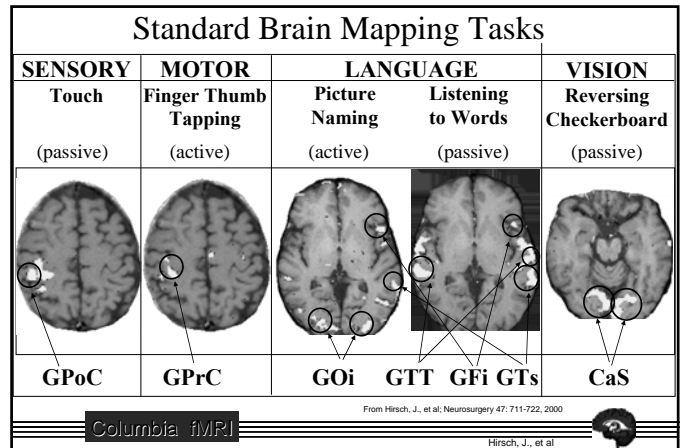
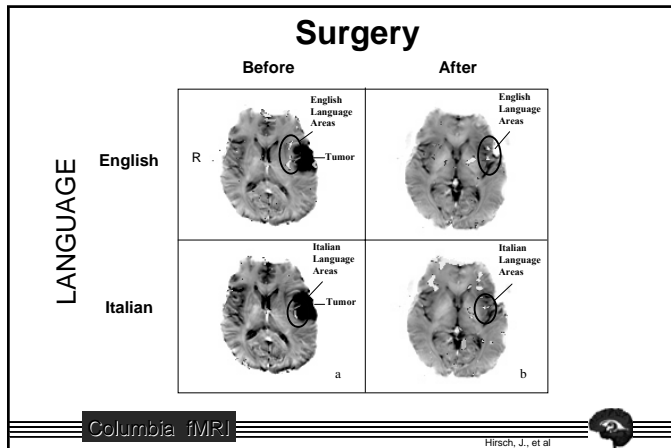
- ## II. Brain Mapping Techniques
- ### B. Cardiovascular Based Methods
1. Positron Emission Tomography, PET
 2. Functional Magnetic Resonance Imaging, fMRI
 - a. Source of signal
 - b. Measurement techniques
 - c. Computation for analysis
 - d. Individual brain maps
- Columbia fMRI Hirsch, J., et al

Mapping Specific Functions to Locate Specific Areas

Brain Mapping and Neurosurgery: [Fixed Effects]

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II. Brain Mapping Techniques

C. Electromagnetic - Based Methods

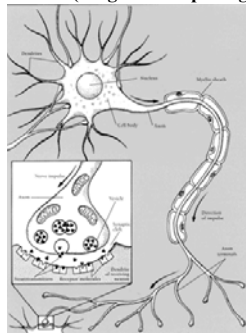
- Somatosensory Evoked Potential, SSEP
- Direct Cortical Stimulation
- Magnetoencephalography, MEG
 - a. Source of signal

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Methods to Measure Electromagnetic Activity:

MEG (Magnetoencephalography) - EEG (Electroencephalography)



- Signal Source: Electrical Activity of nerve cells.
- What is measured on the surface of the head is the result of mostly postsynaptic potentials (excitatory or inhibitory)
- Many nerve cells are aligned in palisades (e.g. pyramidal cells) and post-synaptic electrical fields sum with increasing area.
- Typically it is thought that 100,000 adjacent neurons acting in temporal synchrony are required to produce a measurable change in the magnetic field

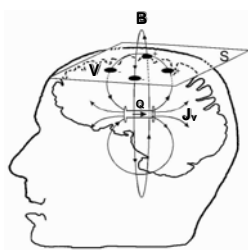
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Relationship between currents in the brain and the magnetic field outside the head.

○ Based on the discovery that electrical currents generate magnetic fields: Hans Christian Oersted, a Danish physicist (early 19th. century)

○ A current source with strength Q causes a current flow J_v within the brain.



○ The current flow produces a potential difference V on the scalp: (measured by EEG)

○ And a magnetic field B outside of the head: (measured by MEG)

from:
www.Aston.ac.uk/psychology/meg/meg/intro/magfield.htm

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II. Brain Mapping Techniques

C. Electromagnetic - Based Methods

- Somatosensory Evoked Potential, SSEP
- Direct Cortical Stimulation
- Magnetoencephalography, MEG
 - a. Source of signal
 - b. Measurement techniques

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Magnetoencephalography, MEG

Tiny magnetic fields produced by brain activity (10^{-13} Teslas) can be measured using Superconducting Quantum Interference Devices (SQUIDS).



SQUIDS operate at superconducting temperatures (-269°C). Sensors are placed in a dewar containing liquid helium.

Stimulus - evoked neuromagnetic signals are recorded by an array of detectors.

The spatial location of the source is inferred by mathematical modeling of the magnetic field pattern.

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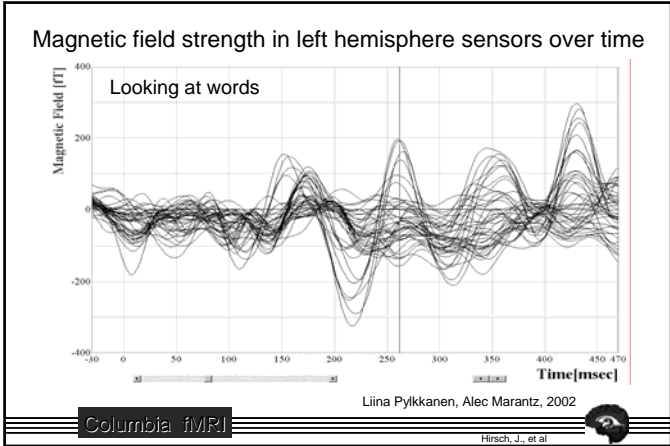
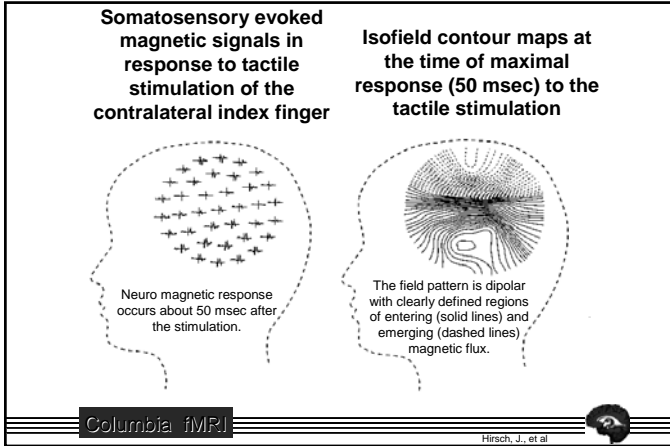
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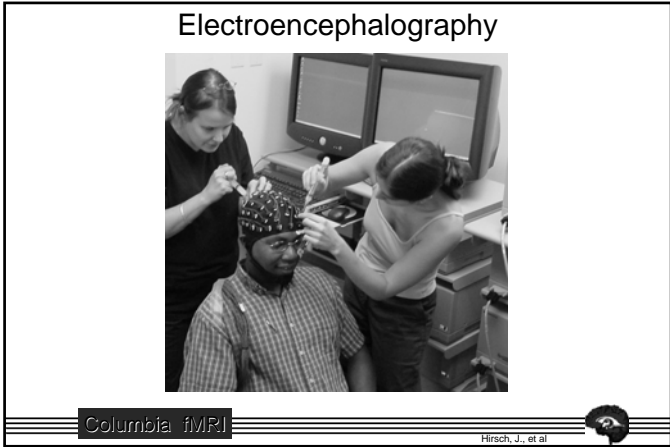
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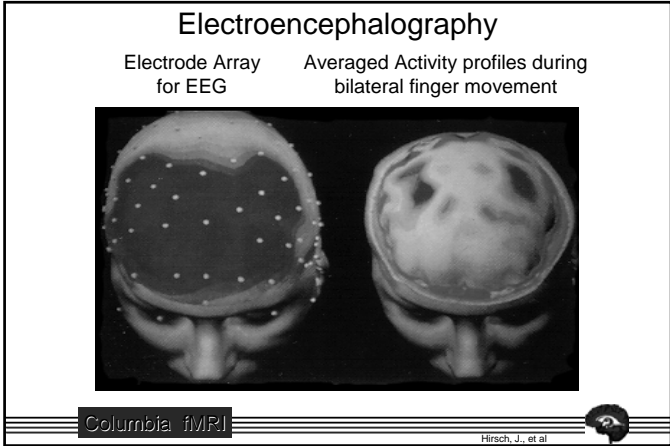
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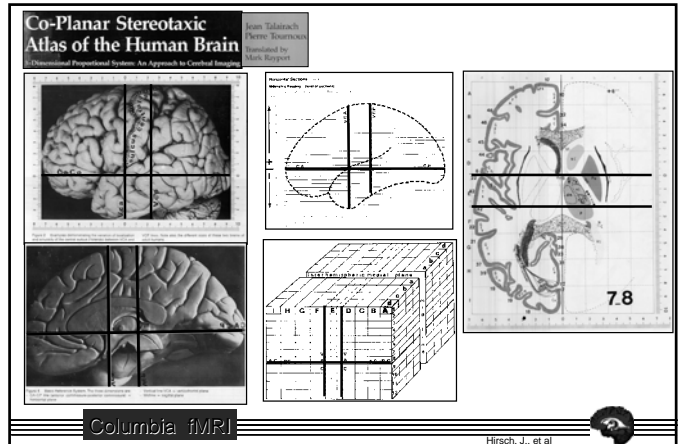
C. Integration of Brain Mapping Technique

Mapping specific functions to understand a neural system

- Normalized Brain
- Inferences to general population [Random effects]

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Labeling of Active Brain Areas

Functional Brain

Atlas Brain



activity

transfer

labels

| Name | BA | Sector |
|------|----|-----------|
| GPrC | 4 | c,E |
| GFs | 6 | b,E |
| GFd | 6 | a,E,60,-a |
| GFs | 6 | b,E,60 |
| GRC | 4 | c,E,60 |
| LPs | 7 | b,G,60 |

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| Anatomical Region | BA | Center of mass | | |
|-------------------------|----|----------------|-----|----|
| | | x | y | z |
| Medial Frontal Gyrus | 6 | 9 | -6 | 53 |
| Superior Temporal Gyrus | 22 | 57 | -28 | 9 |
| Inferior Frontal Gyrus | 44 | 49 | 10 | 25 |
| Inferior Frontal Gyrus | 45 | 40 | 25 | 8 |

Hirsch, R-Moreno, Kim. Interconnected large-scale systems for three fundamental cognitive tasks revealed by functional MRI. Journal of Cognitive Neuroscience, 13(3), 389-405, 2001.

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Functional MRI Research Center

Department of Radiology
Center for Neurobiology and Behavior
Columbia University Medical Center

Mission

To establish a collaborative and multi-investigator neuroimaging research environment focused on education, medical applications, and the study of brain, behavior, and therapy-induced cortical effects aimed at the systems of the brain that underlie cognition, perception, and action.

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